



# PCTEST Engineering Laboratory, Inc.

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## CERTIFICATE OF COMPLIANCE (SAR EVALUATION)

Com-Net Ericsson Critical Radio Systems, Inc.  
1 Mountain View Road, Room 2725  
Lynchburg, VA 24502  
Attention: Michael Fulk

Dates of Tests: February 15-16, 2000  
Test Report S/N: SAR.200214067.OWD  
Test Site: PCTEST Lab, Columbia MD

FCC ID

**OWDTR001-EO**

APPLICANT

**Com-Net Ericsson Critical Radio Systems, Inc.**

EUT Type: Part 90 Subpart S - Specialized Mobile Radio (SMR)

Tx Frequency: 806 - 821 MHz (EDAC)

851 - 869 MHz (Talkaround)

Rx Frequency: 851 - 869 MHz (EDAC and Talkaround)

Max. RF Output Power: 3.0 W ERP (34.77 dBm)

Trade Name/Model(s): *ERICSSON EDACS 300P*

FCC Classification: Licensed Non-Broadcast Transmitter Held to Face (TNF)

Application Type: Certification

Serial Number: n/a (pre production)

FCC Rule Part(s): 2.1093; ET Docket 96.326

Modulation: FM

This wireless portable device has been shown to be capable of compliance for localized specific absorption rate (SAR) for uncontrolled environment/general population exposure limits specified in ANSI/IEEE Std. C95.1-1992 and had been tested in accordance with the measurement procedures specified in ANSI/IEEE Std. C95.3-1992. (See Test Report).

I attest to the accuracy of data. All measurements reported herein were performed by me or were made under my supervision and are correct to the best of my knowledge and belief. I assume full responsibility for the completeness of these measurements and vouch for the qualifications of all persons taking them.

NVLAP accreditation does not constitute any product endorsement by NVLAP or any agency of the United States Government.

PCTEST certifies that no party to this application has been denied the FCC benefits pursuant to Section 5301 of the Anti-Drug Abuse Act of 1988, 21 U.S.C. 853(a).

  
Randy Ortanez  
President & Chief Engineer

**200214067. OWD**



**NVLAP**<sup>®</sup>  
LAB CODE 100431-0

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# SAR MEASUREMENT REPORT

## 1.1 Scope

*Environmental evaluation measurements of specific absorption rate<sup>1</sup> (SAR) distributions in simulated human tissues exposed to radiofrequency (RF) radiation from wireless portable devices for compliance with the rules and regulations of the U.S. Federal Communications Commission (FCC).<sup>2</sup>*

Applicant Name:	Com-Net Ericsson Critical Radio Systems, Inc.
Address:	1 Mountain View Road, Room 2725
Attention:	Lynchburg, VA 24052
	Michael Fulk

- EUT Type: Part 90 Subpart S - Specialized Mobile Radio (SMR)
- Trade Name: ERICSSON
- Model(s): EDACS 300P
- FCC IDENTIFIER: OWDTR001-E0
- S/N: Pre-production
- Tx Frequency: 806 – 821 MHz (EDAC)  
851 – 869 MHz (Talkaround)
- Rx Frequency : 851 – 869 MHz  
(EDAC and Talkaround)
- Application Type: Certification
- FCC Classification: Licensed Non-Broadcast  
Transmitter Held to Face (TNF)
- Modulation(s): FM
- FCC Rule Part(s): § 2.1093, Docket 96-326
- Max. RF Output Power: 3.0 W ERP (34.77 dBm)
- Antenna Type: Antenna No. 1: Helical ( $\lambda/2$ )  
Antenna No. 2: Helical ( $\lambda/4$ )
- Dates of Tests: February 15-16, 2000
- Place of Tests: PCTEST Engineering Lab.  
Columbia, MD, U.S.A.
- Report Serial No.: SAR.200214067.OWD



Fig. 1 SAR Test Setup



<sup>1</sup> Specific Absorption Rate (SAR) is a measure of the rate of energy absorption due to exposure to an RF transmitting source (wireless portable device).

<sup>2</sup> IEEE/ANSI Std. C95.1-1992 limits are used to determine compliance with FCC ET Docket 93-62.

## 2.1 INTRODUCTION

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The FCC has adopted the guidelines for evaluating the environmental effects of radiofrequency radiation in ET Docket 93-62 on Aug. 6, 1996 to protect the public and workers from the potential hazards of RF emissions due to FCC-regulated portable devices.[1]

The safety limits used for the environmental evaluation measurements are based on the criteria published by the American National Standards Institute (ANSI) for localized specific absorption rate (SAR) in *IEEE/ANSI C95.1-1992 Standard for Safety Levels with Respect to Human Exposure to Radio Frequency Electromagnetic Fields, 3 kHz to 300 GHz*. (c) 1992 by the Institute of Electrical and Electronics Engineers, Inc., New York, New York 10017.[2] The measurement procedure described in *IEEE/ANSI C95.3-1992 Recommended Practice for the Measurement of Potentially Hazardous Electromagnetic Fields - RF and Microwave*[3] is used for guidance in measuring SAR due to the RF radiation exposure from the Equipment Under Test (EUT). These criteria for SAR evaluation are similar to those recommended by the National Council on Radiation Protection and Measurements (NCRP) in *Biological Effects and Exposure Criteria for Radiofrequency Electromagnetic Fields*, NCRP Report No. 86 (c) NCRP, 1986, Bethesda, MD 20814.[4] SAR is a measure of the rate of energy absorption due to exposure to an RF transmitting source. SAR values have been related to threshold levels for potential biological hazards.

## 2.2 SAR Definition

Specific Absorption Rate (SAR) is defined as the time derivative (rate) of the incremental energy ( $dU$ ) absorbed by (dissipated in) an incremental mass ( $dm$ ) contained in a volume element ( $dV$ ) of a given density ( $r$ ). It is also defined as the rate of RF energy absorption per unit mass at a point in an absorbing body (see Fig. 2).

$$SAR = \frac{d}{dt} \left( \frac{dU}{dm} \right) = \frac{d}{dt} \left( \frac{dU}{r dV} \right)$$

Figure 1. SAR Mathematical Equation

**SAR is expressed in units of Watts per Kilogram (W/kg).**

$$SAR = s E^2 / r$$

where:

**s** = conductivity of the tissue-simulant material (S/m)

**r** = mass density of the tissue-simulant material (kg/m<sup>3</sup>)

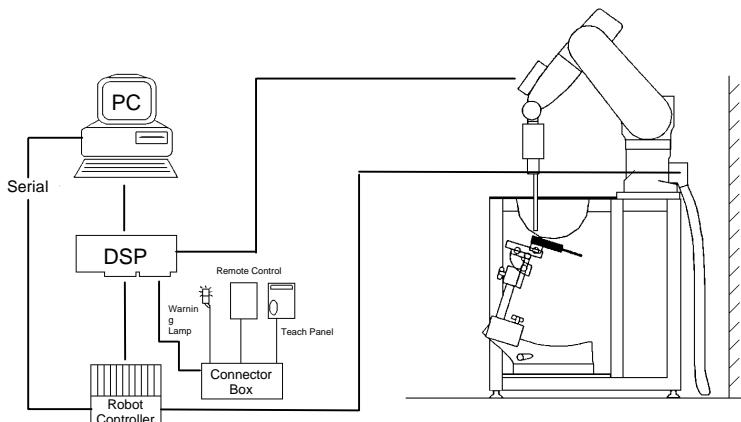
**E** = Total RMS electric field strength (V/m)

NOTE: The primary factors that control rate of energy absorption were found to be the wavelength of the incident field in relations to the dimensions and geometry of the irradiated organism, the orientation of the organism in relation to the polarity of field vectors, the presence of reflecting surfaces, and whether conductive contact is made by the organism with a ground plane.[4]

### **3.1 SAR MEASUREMENT SET-UP**

These measurements are performed using the DASY3 automated dosimetric assessment system. It is made by Schmid & Partner Engineering AG (SPEAG) in Zurich, Switzerland. It consists of high precision robotics system (Staubli), robot controller, Pentium III computer, near-field probe, probe alignment sensor, and the generic twin phantom containing the brain or muscle equivalent material. The robot is a six-axis industrial robot performing precise movements to position the probe to the location (points) of maximum electromagnetic field (EMF) (see Fig. 2).

A cell controller system contains the power supply, robot controller, teach pendant (joystick), and remote control, is used to drive the robot motors. The PC consists of the Micron Pentium III 500 MHz computer with Windows NT system and SAR Measurement Software DASY3, A/D interface card, monitor, mouse, and keyboard. The Staubli Robot is connected to the cell controller to allow software manipulation of the robot. A data acquisition electronic (DAE) circuit performs the signal amplification, signal multiplexing, AD-conversion, offset measurements, mechanical surface detection, collision detection, etc. is connected to the Electro-optical coupler (EOC). The EOC performs the conversion from the optical into digital electric signal of the DAE and transfers data to the PC plug-in card. The DAE3 consists of a



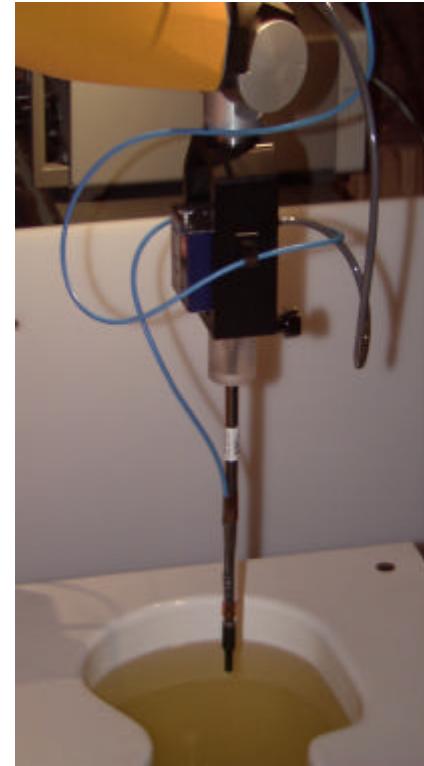
**Figure 2. PCTEST SAR Lab II Test Measurement Set-up**

highly sensitive electrometer-grade preamplifier with auto-zeroing, a channel and gain-switching multiplexer, a fast 16 bit AD-converter and a command decoder and control logic unit. Transmission to the PC-card is accomplished through an optical downlink for data and status information and an optical uplink for commands and clock lines. The mechanical probe mounting device includes two different sensor systems for frontal and sidewise probe contacts. They are also used for mechanical surface detection and probe collision detection. The robot uses its own controller with a built in VME-bus computer. The system is described in detail in [5].

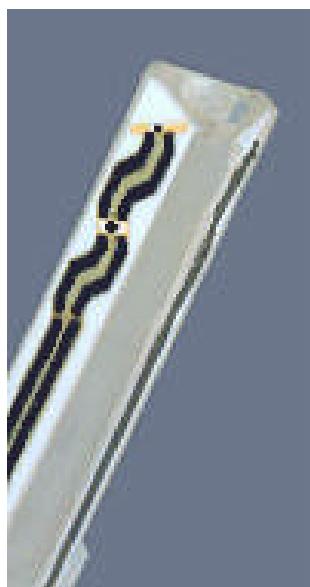
## 4.1 DASY3 E-FIELD PROBE SYSTEM

### 4.2 ET3DV5 Probe Specification

Construction	Symmetrical design with triangular core Built-in optical fiber for surface detection System Built-in shielding against static charges
Calibration	In air from 10 MHz to 2.5 GHz In brain and muscle simulating tissue at Frequencies of 450 MHz, 900 MHz and 1.8 GHz (accuracy $\pm$ 8%)
Frequency	10 MHz to > 6 GHz; Linearity: $\pm$ 0.2 dB (30 MHz to 3 GHz)
Directivity	$\pm$ 0.2 dB in brain tissue (rotation around probe axis) $\pm$ 0.4 dB in brain tissue (rotation normal probe axis)
Dynamic Range	5 $\mu$ W/g to > 100 mW/g; Linearity: $\pm$ 0.2 dB
Surface Detection	$\pm$ 0.2 mm repeatability in air and clear liquids over diffuse reflecting surfaces.
Dimensions	Overall length: 330 mm Tip length: 16 mm Body diameter: 12 mm Tip diameter: 6.8 mm Distance from probe tip to dipole centers: 2.7 mm
Application	General dosimetry up to 3 GHz Compliance tests of mobile phones Fast automatic scanning in arbitrary phantoms



**Figure 4. Photograph of the Probe and the Phantom**



**Fig. 5. ET3DV5 E-field Probe**

The SAR measurements were conducted with the dosimetric probe ET3DV5, designed in the classical triangular configuration [5] and optimized for dosimetric evaluation. The probe is constructed using the thick film technique; with printed resistive lines on ceramic substrates. The probe is equipped with an optical multifiber line ending at the front of the probe tip. It is connected to the EOC box on the robot arm and provides an automatic detection of the phantom surface. Half of the fibers are connected to a pulsed infrared transmitter, the other half to a synchronized receiver. As the probe approaches the surface, the reflection from the surface produces a coupling from the transmitting to the receiving fibers. This reflection increases first during the approach, reaches a maximum and then decreases. If the probe is flatly touching the surface, the coupling is zero. The distance of the coupling maximum to the surface is independent of the surface reflectivity and largely independent of the surface to probe angle. The DASY3 software reads the reflection during a software approach and looks for the maximum using a 2<sup>nd</sup> order fitting. The approach is stopped at reaching the maximum.

## 5.1 E-FIELD PROBE CALIBRATION PROCESS

### 5.2 E-Probe Calibration

Each probe is calibrated according to a dosimetric assessment procedure described in [6] with an accuracy better than +/- 10%. The spherical isotropy was evaluated with the procedure described in [7] and found to be better than +/- 0.25dB. The sensitivity parameters (NormX, NormY, NormZ), the diode compression parameter (DCP) and the conversion factor (ConvF) of the probe is tested.

The free space E-field from amplified probe outputs is determined in a test chamber. This is performed in a TEM cell for frequencies below 1 GHz, and in a waveguide above 1 GHz for free space. For the free space calibration, the probe is placed in the volumetric center of the cavity and at the proper orientation with the field. The probe is then rotated 360 degrees.

E-field temperature correlation calibration is performed in a flat phantom filled with the appropriate simulating tissue. The measured free space E-field in the medium correlates to temperature rise in a dielectric medium. For temperature correlation calibration a RF transparent thermistor-based temperature probe is used in conjunction with the E-field probe.

$$\text{SAR} = C \frac{\Delta T}{\Delta t}$$

where:

$\Delta t$  = exposure time (30 seconds),

$C$  = heat capacity of tissue (brain or muscle),

$\Delta T$  = temperature increase due to RF exposure.

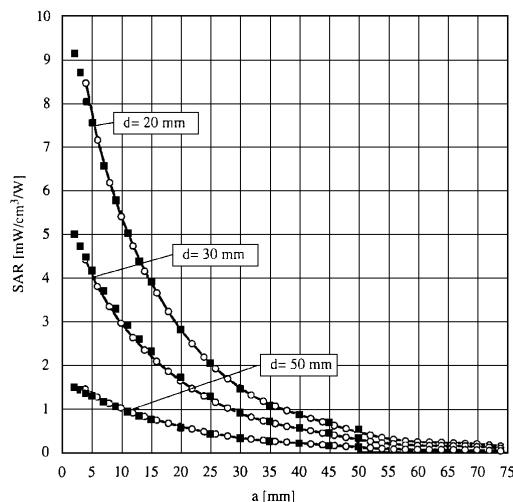
SAR is proportional to  $\Delta T / \Delta t$ , the initial rate of tissue heating, before thermal diffusion takes place. Now it's possible to quantify the electric field in the simulated tissue by equating the thermally derived SAR to the E-field;

$$\text{SAR} = \frac{|\mathbf{E}|^2 \cdot \rho}{r}$$

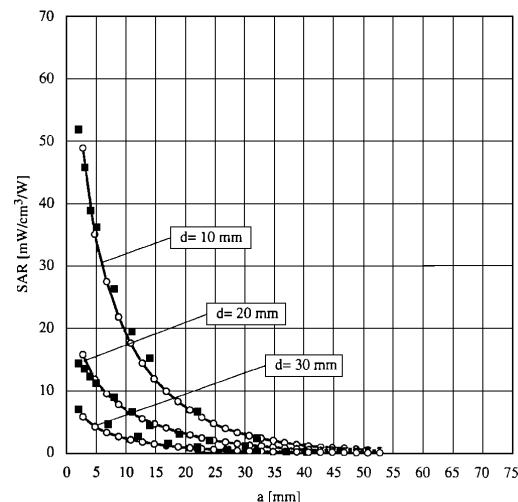
where:

$\rho$  = simulated tissue conductivity,

$\rho$  = Tissue density (1.25 g/cm<sup>3</sup> for brain tissue)



**Figure 6. E-Field and Temperature measurements at 900MHz [5]**



**Figure 7. E-Field and temperature measurements at 1.8GHz [5]**

## 5.3 Data Extrapolation

The DASY3 software automatically executes the following procedures to calculate the field units from the microvolt readings at the probe connector. The first step of the evaluation is a linearization of the filtered input signal to account for the compression characteristics of the detector diode. The compensation depends on the input signal, the diode type and the DC-transmission factor from the diode to the evaluation electronics. If the exciting field is pulsed, the crest factor of the signal must be known to correctly compensate for peak power. The formula for each channel can be given as [8]:

$$V_i = U_i + U_i^2 \cdot \frac{cf}{dcp_i} \quad \text{with} \quad \begin{aligned} V_i &= \text{compensated signal of channel } i \quad (i=x,y,z) \\ U_i &= \text{input signal of channel } i \quad (i=x,y,z) \\ cf &= \text{crest factor of exciting field} \quad (\text{DASY parameter}) \\ dcp_i &= \text{diode compression point} \quad (\text{DASY parameter}) \end{aligned}$$

From the compensated input signals the primary field data for each channel can be evaluated:

E-field probes:

$$E_i = \sqrt{\frac{V_i}{Norm_i \cdot ConvF}} \quad \text{with} \quad \begin{aligned} V_i &= \text{compensated signal of channel } i \quad (i = x,y,z) \\ Norm_i &= \text{sensor sensitivity of channel } i \quad (i = x,y,z) \\ &\mu\text{V}/(\text{V}/\text{m})^2 \text{ for E-field probes} \\ ConvF &= \text{sensitivity of enhancement in solution} \\ E_i &= \text{electric field strength of channel } i \text{ in } \text{V}/\text{m} \end{aligned}$$

The RSS value of the field components gives the total field strength (Hermetian magnitude):

$$E_{tot} = \sqrt{E_x^2 + E_y^2 + E_z^2}$$

The primary field data are used to calculate the derived field units.

$$SAR = E_{tot}^2 \cdot \frac{\sigma}{r \cdot 1000} \quad \text{with} \quad \begin{aligned} SAR &= \text{local specific absorption rate in } \text{W}/\text{g} \\ E_{tot} &= \text{total field strength in } \text{V}/\text{m} \\ \sigma &= \text{conductivity in } [\text{mho}/\text{m}] \text{ or } [\text{Siemens}/\text{m}] \\ \rho &= \text{equivalent tissue density in } \text{g}/\text{cm}^3 \end{aligned}$$

The power flow density is calculated assuming the excitation field to be a free space field.

$$P_{pwe} = \frac{E_{tot}^2}{3770} \quad \text{with} \quad \begin{aligned} P_{pwe} &= \text{equivalent power density of a plane wave in } \text{W}/\text{cm}^2 \\ E_{tot} &= \text{total electric field strength in } \text{V}/\text{m} \end{aligned}$$

## 6.1 PHANTOM, HOLDER AND THE EQUIVALENT TISSUES

### 6.2 Generic Twin Phantom

The Generic Twin Phantom is constructed of a fiberglass shell integrated in a wooden table. The shape of the shell is based on data from an anatomical study designed to determine the maximum exposure in at least 90% of all users [9][10]. It enables the dosimetric evaluation of left and right hand phone usage as well as body mounted usage at the flat phantom region. A cover prevents the evaporation of the liquid. Reference markings on the Phantom allow the complete setup of all predefined phantom positions and measurement grids by manually teaching three points in the robot. See Figure 8.



Shell Thickness	2 ± 0.1 mm
Filling Volume	Volume Approx. 20 liters
Dimensions	810 x 1000 x 500 mm (H x L x W)

Fig. 8 Generic Twin Phantom

### 6.3 Tissue Simulating Mixture Characterization

The mixtures consist of a viscous gel using hydroxethylcellulose (HEC) gelling agent and saline solution (see Table 1). Preservation with a bacteriocide is added and visual inspection is made to make sure air bubbles are not trapped during the mixing process. The mixture is calibrated to obtain proper dielectric constant (permittivity) and conductivity of brain or muscle tissue. The mixture characterizations used for the tissue simulating liquids are according to the data by C. Gabriel and G. Hartsgrove [11].

MIXTURE %	FREQUENCY (Brain) 800 - 850 MHz	FREQUENCY (Muscle) 800 -850 MHz
		800 -850 MHz
WATER	40.4	52.4
SUGAR	56.0	45.0
SALT	2.5	1.4
BACTERIACIDE	0.1	0.2
HEC	1.0	1.0

Table 1. Composition of the Tissue Equivalent Matters

### 6.4 Device Holder for Transmitters

In combination with the Generic Twin Phantom V3.0, the Mounting Device (POM) enables the rotation of the mounted transmitter in spherical coordinates whereby the rotation points is the ear opening. The devices can be easily, accurately, and repeatably positioned according to the FCC and CENELEC specifications. The device holder can be locked at different phantom locations (left head, right head, flat phantom).



Fig. 9. Device Holder

\* Note: A simulating human hand is not used due to the complex anatomical and geometrical structure of the hand that may produce infinite number of configurations [10]. To produce the worst-case condition (the hand absorbs antenna output power), the hand is omitted during the tests.

## 7.1 SYSTEM SPECIFICATIONS

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### 7.2 Robotic System Specifications

#### Specifications

**POSITIONER:** Stäubli Unimation Corp. Robot Model: RX60L  
**Repeatability:** 0.02 mm  
**No. of axis:** 6

#### Data Acquisition Electronic (DAE) System

##### Cell Controller

**Processor:** Pentium III  
**Clock Speed:** 450 MHz  
**Operating System:** Windows NT  
**Data Card:** DASY3 PC-Board

##### Data Converter

**Features:** Signal Amplifier, multiplexer, A/D converter, and control logic  
**Software:** DASY3 software  
**Connecting Lines:** Optical downlink for data and status info.  
Optical uplink for commands and clock

#### PC Interface Card

**Function:** 24 bit (64 MHz) DSP for real time processing  
Link to DAE3  
16 bit A/D converter for surface detection system  
serial link to robot  
direct emergency stop output for robot

#### E-Field Probes

**Model:** ET3DV5      S/N: 1368      S/N: 1370  
**Construction:** Triangular core fiber optic detection system  
**Frequency:** 10 MHz to 6 GHz  
**Linearity:**  $\pm 0.2$  dB (30 MHz to 3 GHz)

#### Phantom

**Phantom:** Generic Twin  
**Shell Material:** Fiberglass  
**Thickness:** 2.0  $\pm$  0.1 mm

#### Tissue Parameters

	800-850 MHz (Brain)	800-850 MHz (Muscle)
Dielectric Constant: $\epsilon$	42.5	56.2
Conductivity: $\sigma$	0.86	0.95

## 8.1 MEASUREMENT PROCESS

### 8.2 System Verification

Prior to assessment, the system is verified to the  $\pm 5\%$  of the specifications by using the system validation kit. (Graphics plots attached)

Validation Kit	Muscle	Targeted SAR <sub>1g</sub> (mW/g)	Measured SAR <sub>1g</sub> (mW/g)
D835V2, S/N: 406		2.11	2.20

### 8.3 Dosimetric Assessment Setup

The evaluation was performed with the following procedure:

1. The SAR value at a fixed location above the ear point was measured and was used as a reference value for assessing the power drop.
2. The SAR distribution at the exposed side of the head was measured at a distance of 3.9mm from the inner surface of the shell. The area covered the entire dimension of the head and the horizontal grid spacing was 20mm x 20mm. Based on this data, the area of the maximum absorption was determined by spline interpolation.
3. Around this point, a volume of 32mm x 32mm x 34mm was assessed by measuring 5 x 5 x 7 points. On this basis of this data set, the spatial peak SAR value was evaluated with the following procedure:
  - a. The data at the surface were extrapolated, since the center of the dipoles is 2.7mm away from the tip of the probe and the distance between the surface and the lowest measuring point is 1.2mm. The extrapolation was based on a least square algorithm [13]. A polynomial of the fourth order was calculated through the points in z-axes. This polynomial was then used to evaluate the points between the surface and the probe tip.
  - b. The maximum interpolated value was searched with a straight-forward algorithm. Around this maximum the SAR values averaged over the spatial volumes (1g or 10g) were computed using the 3D-Spline interpolation algorithm. The 3D-spline is composed of three one-dimensional splines with the "Not a knot" condition (in x, y, and z directions) [13][14]. The volume was integrated with the trapezoidal algorithm. One thousand points (10 x 10 x 10) were interpolated to calculate the average.
  - c. All neighboring volumes were evaluated until no neighboring volume with a higher average value was found.
4. The SAR value, at the same location as procedure #1, was re-measured. If the value changed by more than 5%, the evaluation is repeated.

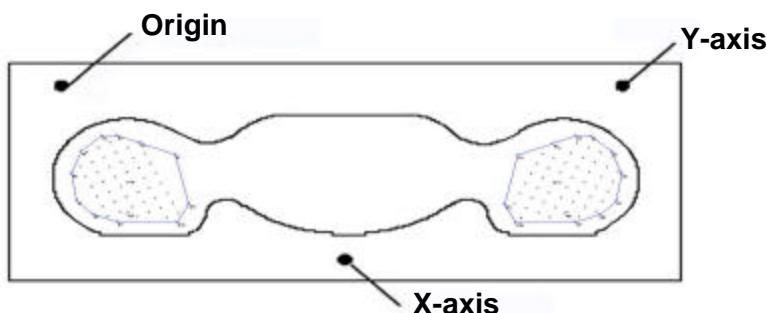


Fig 10. SAR Measurement Points in Area Scan

## **9.1 TEST POSITION OF THE RADIO**

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### **9.2 FACE-HELD TEST SETUP**

The radio was placed in a normal operating position with the center of the mouthpiece aligned with the mouth and parallel to the face of the phantom (See figure 8.) Testing is performed with the use of a head/torso, or flat phantom, as applicable, filled with a muscle equivalent tissue. SAR test is then performed in antenna in and out (if applicable), or fixed antenna position using the low, middle and high channels.



Figure 8. Diagram showing typical alignment of radio held to face.

## 10.1 ANSI/IEEE C95.1 - 1992 RF EXPOSURE LIMITS

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HUMAN EXPOSURE	UNCONTROLLED ENVIRONMENT General Population (W/kg) or (mW/g)	CONTROLLED ENVIRONMENT Occupational (W/kg) or (mW/g)
<b>SPATIAL PEAK SAR *</b> (Brain)	1.60	8.00
<b>SPATIAL AVERAGE SAR **</b> (Whole Body)	0.08	0.40
<b>SPATIAL PEAK SAR ***</b> (Hands / Feet / Ankle / Wrist)	4.00	20.00

Table 2. Safety Limits for Partial Body Exposure [2]

**NOTES:**

\* The Spatial Peak value of the SAR averaged over any 1 gram of tissue (defined as a tissue volume in the shape of a cube) and over the appropriate averaging time.

\*\* The Spatial Average value of the SAR averaged over the whole-body.

\*\*\* The Spatial Peak value of the SAR averaged over any 10 grams of tissue (defined as a tissue volume in the shape of a cube) and over the appropriate averaging time.

**Uncontrolled Environments** are defined as locations where there is the exposure of individuals who have no knowledge or control of their exposure.

**Controlled Environments** are defined as locations where there is exposure that may be incurred by persons who are aware of the potential for exposure, (i.e. as a result of employment or occupation).

## **11.1 MEASUREMENT UNCERTAINTIES**

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Measurement uncertainties in SAR measurements are difficult to quantify due to several variables including biological, physiological, and environmental. However, we estimate the measurement uncertainties in SAR to be less than 15-25 % [16].

According to ANSI/IEEE C95.3, the overall uncertainties are difficult to assess and will vary with the type of meter and usage situation. However, accuracy's of  $\pm 1$  to  $3$  dB can be expected in practice, with greater uncertainties in near-field situations and at higher frequencies (shorter wavelengths), or areas where large reflecting objects are present. Under optimum measurement conditions, SAR measurement uncertainties of at least  $\pm 2$ dB can be expected.[3]

According to CENELEC [17], typical worst-case uncertainty of field measurements is  $\pm 5$  dB. For well-defined modulation characteristics the uncertainty can be reduced to  $\pm 3$  dB.

<b>Uncertainty Description</b>	<b>Error</b>	<b>Distribution</b>	<b>Weight</b>	<b>Std. Deviation</b>	<b>Offset</b>
<b>Probe Uncertainty</b>					
Axial isotropy	$\pm 0.2$ dB	U-Shaped	0.5	$\pm 2.4$ %	
Spherical isotropy	$\pm 0.4$ dB	U-Shaped	0.5	$\pm 4.8$ %	
Isotropy from gradient	$\pm 0.5$ dB	U-Shaped	0	$\pm$	
Spatial resolution	$\pm 0.5$ %	Normal	1	$\pm 0.5$ %	
Linearity error	$\pm 0.2$ dB	Rectangle	1	$\pm 2.7$ %	
Calibration error	$\pm 3.3$ %	Normal	1	$\pm 3.3$ %	
<b>SAR Evaluation Uncertainty</b>					
Data acquisition error	$\pm 1$ %	Rectangle	1	$\pm 0.6$ %	
ELF and RF disturbances	$\pm 0.25$ %	Normal	1	$\pm 0.25$ %	
Conductivity assessment	$\pm 10$ %	Rectangle	1	$\pm 5.8$ %	
<b>Spatial Peak SAR Evaluation Uncertainty</b>					
Extrapolated boundary effect	$\pm 3$ %	Normal	1	$\pm 3$ %	$\pm 5$ %
Probe positioning error	$\pm 0.1$ mm	Normal	1	$\pm 1$ %	
Integrated and cube orientation	$\pm 3$ %	Normal	1	$\pm 3$ %	
Cube Shape inaccuracies	$\pm 2$ %	Rectangle	1	$\pm 1.2$ %	
Device positioning	$\pm 6$ %	Normal	1	$\pm 6$ %	
<b>Combined Uncertainties</b>				$\pm 11.7$ %	$\pm 5$ %

**Table 3. Breakdown of Errors [18]**

## 12.1 SAR TEST DATA SUMMARY

Ambient TEMPERATURE (°C) \_\_\_\_\_ 22.0  
Relative HUMIDITY (%) \_\_\_\_\_ 62.0  
Atmospheric PRESSURE (kPa) \_\_\_\_\_ 100.4

Mixture Type: \_\_\_\_\_ Muscle

Dielectric Constant: \_\_\_\_\_ 56.2

Conductivity: \_\_\_\_\_ 0.95 S/m

### 12.3 Measurement Results (Mouth SAR)

Frequency		Modulation	Power* (W)	Separation Distance (cm)	Antenna No.**	SAR (W/kg)
MHz	Ch.					
806.02500	01	FM	3.0	5.0	1	0.775
821.01250	04	FM	3.0	5.0	1	0.793
858.1500	07	FM	3.0	5.0	1	0.598
805.0250	01	FM	3.0	5.0	2	0.845
821.0125	04	FM	3.0	5.0	2	0.921
858.1500	07	FM	3.0	5.0	2	0.618
<b>ANSI / IEEE C95.1 1992 - SAFETY LIMIT Spatial Peak (Muscle) Uncontrolled Exposure/General Population</b>				<b>Mouth/Face 1.6 W/kg (mW/g)</b> averaged over 1 gram		

#### NOTES:

1. All modes of operation were investigated and the worst-case are reported.
2. Battery condition is fully charged for all readings.
3. Battery  Standard  Extended
4. \*Power Measured  Conducted  EIRP  ERP
5. SAR Measurement System  SPEAG  IDX
6. SAR Configuration  Mouth  Body  Hand
7. \*\*Antenna No. 1 = Helical ( $\lambda/2$ ) Antenna No. 2 = Helical ( $\lambda/4$ )

  
Randy Ortanez  
President & Chief Engineer



Figure 13.  
Mouth SAR Test Setup

## **13.1 SAR TEST EQUIPMENT**

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<b>13.2 Type / Model</b>	<b>Calib. Date</b>	<b>S/N:</b>
Stäubli Robot RX60L	Feb. 00	599131-01
Stäubli Robot Controller	Feb. 00	PCT592
Stäubli Teach Pendant (Joystick)	Feb. 00	3323-00161
Micron Computer 450 MHz Pentium III, Windows NT	Feb. 00	PCT577
SPEAG EDC3	Feb. 00	321
SPEAG DAE3	Feb. 00	330
SPEAG E-Field Probe ET3DV5	Feb. 00	1368
SPEAG E-Field Probe ET3DV5	Feb. 00	1370
SPEAG Dummy Probe	Feb. 00	PCT583
SPEAG Generic Twin Phantom	Feb. 00	PCT587
SPEAG Light Alignment Sensor	Feb. 00	205
SPEAG Validation Dipole D1900V2	Feb. 00	PCT593
Brain Equivalent Matter (800MHz)	Feb. 00	PCTBEM03
Muscle Equivalent Matter (800MHz)	Feb. 00	PCTBEM04
Robot Table		PCT586
Phone Holder		PCT588
A/B Power Indicator		PCT589
Remote Power Switch		PCT590
Phantom Cover		PCT591
HP Spectrum Analyzer	Dec. 99	PCT200
IFI TEM Cell Model: CC110EXX (DC - 2000 MHz)	Jan. 00	A427-0697
Microwave Amp. Model: 5S1G4 (800MHz - 4.2GHz, 5 Watts)	Jan. 00	22332

**NOTE:**

The E-field probe was calibrated by SPEAG. The SAR calibration of the E-field probe is performed by temperature measurement procedure. A TEM cell is used for the free space calibration of the probe. The tissue simulating material is calibrated by PCTEST using the dielectric probe system and network analyzer to determine the conductivity and permittivity (dielectric constant) of the desired equivalent material.

The following list of equipment was used to calibrate the equivalent materials:

Power Meter	Gigatronics 85422
Signal Generator	HP-8648D (9kHz ~ 4GHz)
Power Amp	Amplifier Research 5S1G4 (5 Watts, 800MHz ~ 4.2GHz)
Network Analyzer	HP-8753E (30kHz ~ 3GHz)
Dielectric Probe Kit	HP85070B

## **14.1 CONCLUSION**

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The SAR measurement indicates that the EUT complies with the RF radiation exposure limits of the FCC. These measurements are taken to simulate the RF effects exposure under worst-case conditions. Precise laboratory measures were taken to assure repeatability of the tests.

Please note that the absorption and distribution of electromagnetic energy in the body are very complex phenomena that depend on the mass, shape, and size of the body, the orientation of the body with respect to the field vectors, and the electrical properties of both the body and the environment. Other variables that may play a substantial role in possible biological effects are those that characterize the environment (e.g. ambient temperature, air velocity, relative humidity, and body insulation) and those that characterize the individual (e.g. age, gender, activity level, debilitation, or disease). Because innumerable factors may interact to determine the specific biological outcome of an exposure to electromagnetic fields, any protection guide shall consider maximal amplification of biological effects as a result of field-body interactions, environmental conditions, and physiological variables.[3]

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